

INTERSTITIAL FLUID SAMPLERI. CROSS-REFERENCE TO RELATED APPLICATION

5 The present application discloses and claims
subject matter disclosed in concurrently filed and commonly
assigned U.S. Patent Application Ser. No. _____
entitled "Enhanced Interstitial Fluid Collection".

10 II. BACKGROUND OF THE INVENTION1. Field of the Invention

 This invention pertains to an apparatus for
testing body fluid constituents. More particularly, this
invention pertains to a sampler for use in collecting
15 interstitial fluid.

2. Description of the Prior Art

 In the prior art, there are numerous examples of
apparatus for testing and determining the level of
20 constituents in human blood. A great deal of attention has
been directed to the development of techniques and
apparatus for measuring blood glucose.

 As noted in commonly assigned and co-pending U.S.
Patent Application Nos. 08/321,305 and 08/136,304
25 (corresponding to PCT International Publication
No. WO95/10223 published April 20, 1995 on International
Application No. PCT/US94/11580 and incorporated herein by
reference), the determination of the level of a constituent
of blood can be achieved by measuring the level of that
30 constituent in other body fluids such as interstitial
fluid. The aforementioned patent applications and
international publication disclose a method and apparatus
for a minimally invasive technique for collecting a sample
of interstitial fluid through use of an extremely small
35 needle which penetrates into the dermal layer of the skin
in order to collect a low blood or blood-free sample of

interstitial fluid. The collected interstitial fluid can then be analyzed for a determination of the level of constituents within the fluid. For example, the collected interstitial fluid can be analyzed for an amount of glucose with the determined amount being representative of the amount of glucose contained within the patient's blood.

The aforementioned applications and international publication disclose the use of a ring (item 60 in Fig. 6 of the application) which surrounds the needle to create a pressure area on the patient's skin. It is believed this leads to increase the amount of interstitial fluid being collected.

In the collection of interstitial fluid, it is desirable to increase the speed at which a sample is collected. In the absence of mechanical or other assistance, the rate at which interstitial fluid is collected through a small diameter tube or needle is very slow. Preferably, patients utilizing such equipment for home use, will be provided with a system which collects interstitial fluid at a rapid pace to ensure that a patient does not remove the needle too early in its application. Also, it is important to provide for techniques to increase a volume of interstitial fluid being collected through a needle.

When collecting any body fluid through use of a needle, it is important that the needle be a disposable item in order to prevent re-use of the needle. Such re-use can result in the transmission of disease. Where the apparatus is to be used in a patient's home by the patient, the apparatus should be simple to use and with the needle incorporated in a disposable item. Since the needle is incorporated in a disposable item, it is important that the disposable item be amenable to low-cost manufacture. Also, in order to test the interstitial fluid, the interstitial fluid collection mechanism must be coupled with an analytic

mechanism for analyzing the collected fluid. Where such a device is to be used in home by low-skilled patients, it is important that the sampler and the analytic portion of the device be mutually configured to ensure that the sampler is
5 coupled to the apparatus in a repeatable and reliable manner to minimize errors resulting from use of the apparatus by untrained patients.

III. SUMMARY OF THE INVENTION

10 According to a preferred embodiment of the present invention, a sampler is disclosed for use in an interstitial fluid collection apparatus where the collection apparatus has a light source for generating a testing light and a light detector for detecting light.
15 The light source and the detector are contained within the apparatus in a predetermined alignment to define a light path between the source and the detector. The apparatus further includes an opening of predetermined geometry to define an access to the light path. The sampler includes a
20 main body having a handle and a sample end. The sample end has an external mating geometry which mates with the predetermined geometry of the opening of the apparatus. Therefore, the sample end can be inserted into the opening in a predetermined alignment such that the sampler may be
25 repeatably inserted within the opening in the predetermined alignment with a sample location of the sample end positioned within the light path. An interstitial fluid collection apparatus is carried on the sampler. The interstitial fluid collection apparatus includes a needle
30 sized to protrude beyond the housing. The needle protrudes a distance selected for the needle to penetrate into an interstitial fluid-laden skin layer when the housing is urged against the skin layer by the user. An absorbent medium is carried on the sampler in fluid flow
35 communication with the needle for interstitial fluid to

flow from the needle onto the medium. The medium is positioned at the sample location.

IV. BRIEF DESCRIPTION OF THE DRAWINGS

5 Fig. 1 is a cross-sectional elevation view of an interstitial fluid apparatus showing a sampler contained within the apparatus in a retracted position;

 Fig. 2 is the view of Fig. 1 with the apparatus shown in an extended position;

10 Fig. 3 is a perspective exploded view of the apparatus of Fig. 1;

 Fig. 4 is the view of Fig. 3 rotated 90° to the right of the view of Fig. 3;

 Fig. 5 is the view of Fig. 4 rotated 90° to the
15 right of Fig. 4;

 Fig. 6 is the view of Fig. 5 rotated 90° to the right of Fig. 5;

 Fig. 7 is a perspective view of an optics housing for use in the apparatus of Fig. 1;

20 Fig. 8 is a side elevation view of the housing of Fig. 7;

 Fig. 8A is an enlarged view of a bottom portion of the view of Fig. 8;

 Fig. 9 is a side elevation view of the housing of
25 Fig. 7 rotated 90° from the view of Fig. 8;

 Fig. 10 is a view taken along line 10-10 of Fig. 9;

 Fig. 11 is a bottom plan view of the housing of Fig. 7;

30 Fig. 12 is a perspective view of a shell for use in the apparatus of Fig. 1;

 Fig. 13 is a sectional view of the shell of Fig. 12;

 Fig. 14 is a perspective view of a collar for use
35 in the apparatus of Fig. 1;

Fig. 15 is a sectional view of the collar of
Fig. 14;

Fig. 16 is a perspective view of a base for use
in the apparatus of Fig. 1;

5 Fig. 17 is a sectional view of the base of
Fig. 16;

Fig. 18 is a top, left side and rear end exploded
perspective view of a sampler for use in the apparatus of
Fig. 1;

10 Fig. 19 is a top, left side and rear end
perspective view of a sampler main body for the sampler of
Fig. 18;

Fig. 20 is a left side elevation view of the
sampler main body of Fig. 18 (with the opposite side being
15 substantially identical);

Fig. 21 is a view taken along line 21-21 of
Fig. 20;

Fig. 22 is a view taken along line 22-22 of
Fig. 20;

20 Fig. 23 is an enlarged bottom view of a front
portion of the main body of Fig. 20;

Fig. 24 is a side elevation view of a piston for
the sampler of Fig. 18;

25 Fig. 25 is a view taken along line 25-25 in
Fig. 24;

Fig. 26 is a side elevation view of a catch pin
for the sampler of Fig. 18;

Fig. 27 is a view taken along line 27-27 in
Fig. 26;

30 Fig. 28 is a schematic representation showing the
apparatus of Fig. 1 placed against a patient's skin;

Fig. 29 is the view of Fig. 28 showing initial
forcing of the apparatus against the patient's skin;

35 Fig. 30 is the view of Fig. 28 showing urging of
the apparatus against the patient's skin with penetration

of a needle into the patient's skin layer and with a piston aligned with a pressure ring; and

Fig. 31 is the view of Fig. 28 with the piston protruding beyond the pressure ring.

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V. DESCRIPTION OF THE PREFERRED EMBODIMENT

With reference now to the various drawing figures in which identical elements are numbered identically throughout, a description of the preferred embodiment of
10 the present invention will be shown. While the invention will be described with reference to an apparatus for collecting interstitial fluid to test for glucose within the interstitial fluid, it will be appreciated that the apparatus can be used for testing any body constituent
15 which may be contained within interstitial fluid.

In a preferred embodiment, the apparatus is disclosed with reference to use of a penetrating needle and an absorbing membrane such as that shown and described in U.S. Patent Application Serial Nos. 08/321,305 and
20 08/136,304 (and corresponding PCT International Publication No. WP 95/10223, dated April 20, 1995 on International Application No. PCT/US94/11580; incorporated herein by reference). With reference to Figs. 16-20 of that application (showing a representative embodiment of the
25 invention shown in that application), a needle 214' is surrounded and maintained in fixed relative position by a ring 202'. The ring is placed against a patient's skin in order to define a pressurized area on the patient's skin as the needle 214' penetrates into the skin. The needle is
30 sized to be about 28 to 32 gauge (i.e., .36 mm outside diameter to .23 mm outside diameter) with an anticipated preferred size of about 30 gauge. The needle is made as small as possible to provide a minimally intrusive and painless insertion into the skin. The needle is sized to
35 penetrate into the dermis for a variety of reasons as best

disclosed in the aforementioned application including low pain and the collection of low blood interstitial fluid for subsequent testing. An absorbent membrane 210' is placed in fluid flow communication with the needle 214' such that
5 interstitial fluid which flows through the needle 214' is deposited on the membrane 210' as a spot available for subsequent testing with light (visible or non-visible spectrum). The amount of absorption of various wavelengths of the light indicating the concentration of constituents
10 for testing such as glucose or the like.

The present invention pertains to a testing apparatus which includes a needle 10 disposed in fluid flow communication with an absorbent membrane 12 both in accordance with the teachings of the aforementioned PCT
15 International Publication No. WO95/10223.

The present invention is directed to an apparatus
20 (Figs. 1-6) for collecting and testing interstitial fluid. The apparatus 20 includes a main housing 22 (shown in Figs. 1 and 2 only) coupled to a base 24. The apparatus
20 20 further includes a collar 26 secured to the base 24. A shell 28 is contained within the collar 26. An optics housing 30 is contained within the shell 28. Finally, a sampler 32 is provided to be received within the optics housing 30. Each of base 24, collar 26, shell 28, optics
25 housing 30 and sampler 32 will be separately described.

Main housing 22 is shown only in section in Figs. 1 and 2. Main housing 22 is sized to be gripped by a patient such that the apparatus 20 may be urged against the patient's skin for purpose of collecting interstitial fluid
30 as will be described. In addition to constituting a handle which can be grasped by the patient, the main housing 22 will contain electronics and the like for generating power for a light source as will be described and for analyzing signals from a light detector (as will be described) in
35 order to calculate the level of constituents, such as blood

glucose, contained within a sample of interstitial fluid. Such electronics are not shown but it will be appreciated that such electronics are well within the skill of the art. Examples of circuits for analyzing sampling light are
5 described in commonly assigned U.S. Patent No. 5,115,133 to Knudson dated May 19, 1992 and the aforementioned International Publication No. WO95/10223.

The base 24 is separately shown in Figs. 16 and 17. Base 24 is substantially cylindrical and is provided
10 with an end plate 36 having holes 38 extending at least partially therethrough with the holes 38 sized to receive any suitable fastening means such as bolts or the like for fastening of the end plate 36 to the main housing 22. The base 24 further includes an inner hollow cylinder 40
15 extending from plate 36 with the inner cylinder 40 being coaxial with an outer cylinder 42 of the base 24. Outer cylinder 42 has a threaded inner surface 44.

The collar 26 is separately shown in Figs. 14 and 15. The collar 26 includes an enlarged cylindrical portion
20 50 sized to be received within base 24 and with an end 51 abutting the end plate 36 of base 24. An outer wall 52 is threaded to mate with the internal threading 44 of base 24. An inner wall 53 of cylindrical portion 50 remains spaced from inner cylinder 40 to define a void for receiving
25 springs as will be described (and as shown in Figs. 1-2). The collar 26 also includes a reduced diameter portion 54 with the reduced diameter portion 54 and the enlarged diameter portion 50 connected at an annular stop surface 56 shown in Fig. 15. For purposes that will become apparent,
30 the reduced diameter portion 54 includes a slot 58 at an end 59 of portion 54. Linearly aligned with slot 58 is a hole 61.

The shell 28 is separately shown in Figs. 12 and 13. The shell 28 includes a cylindrical body 60 sized to
35 be slidably received in close tolerance within the reduced

diameter cylindrical portion 54 of collar 26. The cylindrical body 60 terminates at a flange 62 positioned to abut stop surface 56 of collar 26. Accordingly, the shell 28 is slidable within the collar 26 with the flange 62
5 movable between the stop surface 56 of collar 26 and the end plate 36 of base 24.

The cylindrical body 60 has at its end opposite flange 62 a reduced diameter portion 64 which is coaxial with the main cylindrical body 60. The reduced diameter
10 portion 64 terminates at a first pressure ring 66 with the plane of the opening of the pressure ring 66 being generally perpendicular to the cylindrical axis of body 60. An elongated slot 68 extending generally in the direction of the axis of body 60 is provided extending through the
15 shell 28 with the slot 68 extending substantially the length of the body 60 and substantially the length but not entirely through the sidewall of the reduced diameter portion 64 such that ring 66 is an uninterrupted ring. However, a segmented ring or other incomplete ring would be
20 satisfactory.

The optics housing 30 is separately shown in Figs. 7-11 and includes a generally cylindrical main body 70 (with flat side walls 71a, 71b) having extending axially therefrom a reduced diameter cylinder 72 (surrounded by
25 surface 71) having an annular slot 73. The reduced diameter cylinder 72 is sized to be slidably received within the inner cylinder 40 of base 24 as best shown in Figs. 1 and 2.

The main body 70 includes a first axial slot 74
30 extending partially through a distal end 75 of the body 70. Disposed axially spaced from slot 74 is a second slot 76 extending through the main body 70. A pin receiving hole 77 extends through body 70 perpendicular to slot 76. Ninety degrees offset from slots 74, 76 are access holes 78
35 in communication with a hollow interior 80 of cylinder 72.

Ninety degrees offset from slot 74 are pockets 82, 83 with axes of the pockets 82, 83 in coaxial alignment with one another and in communication with the slot 74. The base end 75 has a ramped ridge 79 extending parallel to hole 77.

5 In the assembly, as best shown in Figs. 1 and 2, a first biasing spring 84 is positioned to act between the base plate 36 of base 24 and the flange 62 of shell 28 urging the shell 28 away from the base plate 36. A second biasing spring 86 is positioned to act against the base
10 plate 36 of base 24 and an engaging surface 71 on cylinder 70 thereby urging the optics housing 30 axially away from the base plate 36.

As shown in Figs. 3-6, a light source 90 is contained within pocket 82. A light detector 92 is
15 contained within pocket 83. Electrical leads (not shown) from both the light source 90 and light detector 92 may be passed between the opposing exterior surfaces 71a, 71b of cylinder 70 and the interior surface of shell cylinder 60 with the leads then passed through the holes 78, into
20 hollow interior 80 of cylinder 72 and directed thus into the circuitry (not shown) contained within the housing 22. The light source 90 and light detector 92 are aligned to define a light path therebetween. The light source 90 generates a testing wavelength. The light detector 92 is
25 selected to measure the intensity of wavelengths including the intensity of the testing wavelength.

A lock pin 94 (shown separately in Figs. 26-27) is contained within optics housing 30 in hole 77 with the lock pin 94 positioned at a 90° angle to the plane of the
30 slot 74. The pin 94 has a ramp 95 disposed in slot 76. In the assembly shown in Figs. 1-6, the slots 74, 76 of the optics housing 30 are in alignment with the slot 68 of the shell 28.

As shown in Figs. 18-25, the sampler 32 includes
35 a body 100 formed of injection molded plastic. The body

100 includes a rear handle portion 101 and a forward sampling portion 102. The handle portion 101 is sized to be gripped by the fingers of a user. At the sampling end 102, the body 100 is provided with a hub or piston 104.
5 The piston 104 is cylindrical and sized to be received in close sliding tolerance within the reduced diameter cylinder 64 of shell 28. The piston terminates at a flat second pressure surface 106 which is generally perpendicular to the axis of the needle 10. While a flat
10 surface 106 is preferred, other shapes (e.g., concave) could be used.

The needle 10 protrudes beyond the surface 106 a distance equal to a desired penetration of the needle 10 into a patient's skin layer. As disclosed in the
15 aforementioned international publication, distance of protrusion of needle 10 is about 1.5 mm to ensure protrusion of the needle 10 into but not through a dermal layer of a patient's skin. At the sampling end 102, the main body 100 is provided with a relief 108 surrounding a
20 hole 110 formed through the body. The hole 110 is in communication with a proximal end 11 of the needle 10. Accordingly, an absorbent material 12 such as the material 210' shown in Figs. 16-20 of the aforementioned International Publication No. WO95/10223 may be placed
25 within the relief 108 such that interstitial fluid which flows up the needle 10 will be deposited upon the membrane 12. The membrane 12 is held in place through any suitable means such as by an adhesive ring 111 (or, alternatively, ultrasonic bonding or other bonding technique).

30 The hole 110 is positioned at a sampling location such that the hole 110 is in the light path between the light source 90 and the light detector 92 when the sampler 32 is placed within the apparatus 20 as will be described. The end 102 is sized to be received within the aligned

slots 68, 74 of shell 28 and optics housing 30, respectively.

The main body 100 is provided with an arcuate rib 113 sized and shaped to abut an exterior surface of the optics housing 30 on both sides of the slot 74 and to curve beneath the base 75. A latching member 112 is connected to the body 100. The latching member 112 pivots at a point of connection to the body 100 and includes a lever arm 114 exposed at the handle portion 101 such that the lever member 114 may be depressed manually by a user. The latch 112 further includes a latching end 116 sized and positioned to be received within the hole 76 of the optics housing 30. The latching end 116 includes a detent 118 (Figs. 1-2) positioned to engage and receive the ramp 95 of the lock pin 94 within the detent 118 when the sampler 32 is inserted within the slots 74, 76 in a predetermined alignment and with the sampling location 110 disposed within the light path between the source 90 and detector 92. A leading end of the locking end 116 is provided with a ramped surface to ride over the pin 94 upon insertion of the sampler 32 within the optics housing 30 and to provide a positive lock as the pin is received within the detent 118. To further secure the sampler 32 in optics housing 30 in the desired alignment, sampler housing 100 has a detent 117 (Fig. 23) to receive ridge 79 on the base 75 of optics housing 30. The sampler 32 may be easily removed by a user depressing end 114 thereby raising end 116 for the pin 94 to clear the detent 118 permitting removal of the sampler 32 from the apparatus.

With the construction thus described, a sampling end 102 may be placed within the aligned slots 74, 68. Over-insertion is avoided by reason of the sampling end 102 butting up against the interior of the optics housing 30. Further, the lock pin 94 received within the detent 118 and the ridge 79 in detent 117 ensure that the sampler 32 is

not under-inserted into the slots 74, 76 by providing a user with a positive feedback indicating that the lock pin 94 has been received within the detent 118 indicating the sampler 32 is in the predetermined alignment. Accordingly, 5 upon receipt of such feedback, the user is assured that the sampling location 110 is in alignment with the light path between the light source 90 and the light detector 92.

The first spring 84 urges the shell away from the base 24 such that the full length of the piston 104 and 10 needle 10 may clear the first pressure ring 66 and be inserted through the slot 68 as the sampler 32 is loaded into apparatus 20.

Due to the locking at detents 118 and 117, sampler 32 is held in a predetermined alignment with the 15 membrane 12 in the light path between light source 90 and light detector 92. To facilitate placement of sampler 32 within apparatus 20, the sampler 32 and apparatus 20 have mating external geometries. Namely, in the rest position of Fig. 1, the shell 28 is fully extended from base 36 by 20 spring 86. Slot 58 of collar 26, slot 68 of shell 28 and slot 74 of optics housing 30 are aligned to permit insertion of end 102 of sampler 32. Further, in this position, slot 68 is sized so that needle 10 may pass ring 66 without interference. Also, in this position, slot 61 25 of collar 26, slot 68 of shell 28 and hole 76 of optics housing 30 are aligned to receive end 116 of lever arm 112.

Upon insertion, the mating geometry of sampler 32 and optics housing 30 insure the membrane 12 is accurately positioned. The ribs 113 acting against the external 30 surface of optics housing 30 together with ribs 95, 79 received within detents 118, 117 securely couple the sampler 32 to optics housing 30 in accurate alignment and with the sampler 32 movable with the optics housing 30. As the optics housing 30 moves relative to shell 28 and collar

26, the sizing of slots 58, 61 and 68 avoid interference with movement of the sampler 32.

Upon initial placement of the apparatus against a patient's skin 200 (Fig. 28), the ring 66 first contacts a patient's skin 200 with the needle 10 being recessed behind the ring 66. Upon urging of the apparatus 20 against the skin 200, the ring 66 moves relative to the needle 10 against the bias of the first spring 84. Upon achieving such relative movement, the needle 10 then penetrates the skin 200 with the second pressure surface 106 of the piston 104 engaging the skin and with both springs 84, 86 resisting further penetration until both springs are compressed. Second spring 86 ensures a constant force acts on piston 106.

Figs. 28-30 show a sequence of operation of the present apparatus. As shown in Fig. 28, during the rest state, the needle 10 is recessed behind the first pressure ring 66 to prevent damage to the needle 10 and inadvertent skin penetration. Upon initial urging of the pressure ring 66 against the skin (Fig. 29), the pressure ring 66 depresses the skin 200 and makes the skin taut in the area defined by the ring 66. Further, the pressurization creates a pressurized area in the zone of the skin layer 200 directly beneath the ring 66. This is desirable since interstitial fluid beneath the skin 200 is believed to exist at a negative pressure. Creating a pressurized zone beneath the ring 66 is believed to assist in rapid collection of interstitial fluid within the needle 10. During this initial pressurization of the skin 200, the ring 66 moves relative to piston 104 until the needle 10 penetrates the skin 200 and the end 106 of the piston 104 abuts the skin 200 (Fig. 30). Further depression (which can occur against soft skin but which may not occur against more rigid skin) is shown in Fig. 31 where the piston end surface 106 protrudes slightly beyond the ring 66 to

further increase the pressure acting in the collection zone of the skin 200 and with full penetration of the needle 10.

It has been found that this sequence of action significantly increases the rate at which interstitial
5 fluid is collected through the needle 10 and deposited on the membrane 12 within the sampler 32.

After full penetration of the needle 10, internal circuitry may then be actuated to operate the light source 92. Absorption of the testing light through the collected
10 sample provides an indication of the amount of the constituent contained on the sample.

In a preferred embodiment, springs 84, 86 are preloaded. Namely, in the rest position of Figs. 1 and 28, first spring 84 exerts an urging force on shell 28 of about
15 three pounds and with a spring constant of about four pounds per inch. Spring 86 is pre-loaded to about one pound and has a spring constant of about two pounds per inch. To accommodate the pre-loading of springs 84, 86, optics housing 30 is provided with a retaining ring 202
20 (shown only in Figs. 1 and 2) in slot 73. The pre-loading of spring 84 insures a minimum skin pressure by ring 66 before penetration of the skin 200 by needle 10.

As shown best in Figs. 1, 2 and 18, membrane 12 is provided with a U-shaped boundary 300. Boundary 300 is
25 formed by ultrasonically or pressure treating membrane 12 to create a material density in boundary 300 which is greater than a material density of the remainder of the membrane 12. Therefore, boundary 300 provides an increased resistance to liquid flow compared to the remainder of the
30 absorbent membrane 12. The end 11 of needle 10 is positioned to deposit interstitial fluid onto the interior of the U-shaped boundary 300. The increased density of the boundary 300 permits the fluid to flow within the interior of the boundary 300 but restricts fluid flow beyond the
35 boundary 300. The target location ("T") of light through

membrane 12 during testing is positioned within the boundary 300. Boundary 300 thus insures that a sufficient volume of collected fluid is in residence at the target location T during testing.

5 It will be appreciated that through use of the present invention the rate at which interstitial fluid is collected through the needle 10 is greatly enhanced over that shown in the aforementioned International Publication No. WO95/10223. Further, the sampling apparatus is
10 contained within a low-cost sampler 32 which can be readily disposed after each use. The mating geometry of the sampler 32 with the internal geometry of the apparatus 20 ensures that the sampler 32 is placed within the apparatus 20 in a predetermined alignment with the sampling location
15 in the light path between the source 90 and the detector 92. The sampling apparatus also ensures a proper positive locking position which may be released easily by an operator and the entire operation of insertion of the sampler within the apparatus and removal of the sampler for
20 subsequent disposal is easily accomplished for a patient.

 Having disclosed the present invention and a preferred embodiment, it will be appreciated that modifications and equivalents of the disclosed concepts may readily occur to one skilled in the art. It is intended
25 that such modifications and equivalents shall be included within the scope of the claims which are appended hereto.